Optimized DCAT for lung and liver SBRT

Rapid and accurate delivery of lung and liver SBRT using optimized dynamic conformal arc treatment (DCAT) with Monaco® treatment planning system and Versa HD™

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Summary

Indications:
- Lung and liver SBRT

Comparison:
- Optimized DCAT versus VMAT
- Delivery efficiency
- Plan quality

Planning and delivery systems:
- Monaco 5.1 with VDR and SSO for DCAT
- Versa HD 6 MV flattening filter free (FFF)

Conclusions
- Comparable plan quality in general
- VMAT is better where OAR are close to/overlap the PTV
- DCAT is comparable/superior where OAR isolated from PTV
- Optimized DCAT can be delivered using 2.5x fewer MU (2.5x faster)
- Monaco DCAT with segment shape optimization (SSO) and variable dose rate (VDR) can be a dosimetrically comparable but more efficient alternative treatment method to VMAT for lung and liver SBRT
Introduction

The introduction and widespread use of intensity modulated radiation therapy (IMRT) in recent decades has enabled improved radiation dose delivery in many cases, allowing better sparing of healthy organs and higher doses to the tumor. But, for targets subject to motion (e.g. respiratory motion), the interplay between the movement of the MLC leaves and the target is a particular concern with IMRT techniques, especially when combined with the ablative doses used in stereotactic body radiation therapy (SBRT). The interplay effect may lead to under-dosage of the target volume or over-dosage of the surrounding healthy tissue.

Recently, there has been renewed interest in the use of dynamic conformal arc therapy (DCAT) for certain SBRT treatments. DCAT reduces the issue of subvolume irradiation because the field aperture is dynamically changed to include the full projection of the target volume at each gantry angle. It has been proposed that the combination of DCAT with SBRT offers shorter treatment times and reduced MLC-target motion interplay effect. But, traditional DCAT does not offer the same level of plan quality that can be achieved using volumetric modulated arc therapy (VMAT).

Traditional DCAT uses a constant dose rate, which can lead to inferior dose distributions compared to VMAT. The dose is skewed higher where the distance to the target is shortest. This is particularly pronounced for targets that are off center axis. To overcome this challenge, Monaco treatment planning system (versions 5.1 and above) has a variable dose rate (VDR) feature for DCAT. VDR optimizes the DCAT delivery by allowing more or less dose to be delivered at any given gantry angle. Monaco changes the segment dose rate or the gantry speed to compensate for beam-to-target differences, which evens out the dose deposition and results in more conformal dose distributions.

Plus, the segment shape optimization (SSO) feature for DCAT in Monaco optimizes beam weights and shapes to enhance organs-at-risk (OAR) sparing and dose conformality. This function allows users to enter goals, constraints and optimization parameters so the planning system can calculate the best plan to meet these objectives. It does this by smoothing and clustering DCAT arc control points, and attributing more or less dose to each segment depending on the location and optimization priority of OAR in the beam path.

The purpose of this study was to assess the plan quality and delivery efficiency of this unique optimized DCAT approach compared to VMAT for lung and liver SBRT.
Method

Nineteen patients, previously treated for lung (n=15) and liver (n=4) lesions with SBRT, were selected for this retrospective study. The Monaco treatment planning system (version 5.1) was used to optimize two SBRT plans for each patient, one using VMAT and one using optimized DCAT. The plans were created for Versa HD with a 6 MV FFF photon beam delivered in two 225-degree arcs.

To ensure that no planning bias was introduced, all OAR and targets were contoured by a single physician and all patient plans were optimized by the same dosimetrist using a common template of PTV and OAR objectives for each of the paired plans without any further optimization. This ensured that all plans were created similarly and consistently.

To control dose fall-off and conform the dose to the target, an auxiliary structure was created for each plan by expanding the PTV by 4 cm. Structures encompassed within the PTV + 4 cm structure were prioritized with higher weights. Objective functions used during plan optimization for a sample case are shown in Table 1.

Delivery efficiency was determined by recording monitor units (MU) for each plan. Plus, two metrics were calculated to compare plan quality: the ratio of PTV to 100 percent isodose volume (PTVr); and, the ratio of PTV to 50 percent isodose volume (R50). PTVr values closer to unity indicate better conformity of the prescription dose to target, while higher R50 values indicate steeper dose fall-off and reduced irradiation of healthy tissue.

Quality assurance

For each plan that was created, a corresponding patient-specific QA plan was also created and delivered to a ScandiDos Delta4 phantom. The gamma index passing rate was calculated with criteria set to two percent and 2 mm for all dose points measured above 10 percent of the maximum dose.

<table>
<thead>
<tr>
<th>Objective name</th>
<th>Objective function</th>
<th>Objective parameters</th>
</tr>
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<tbody>
<tr>
<td>PTV</td>
<td>Target penalty</td>
<td>99% of Rx dose</td>
</tr>
<tr>
<td>PTV + 4 cm</td>
<td>Quadratic overdose</td>
<td>50% of Rx dose 1.2 cm from PTV with 5 cGy RMS</td>
</tr>
<tr>
<td>Ribs</td>
<td>Serial</td>
<td>30 Gy</td>
</tr>
<tr>
<td>Body</td>
<td>Maximum dose</td>
<td>130% of Rx dose</td>
</tr>
</tbody>
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Table 1.
Objective functions used during treatment plan optimization for a sample case
Results

All VMAT and optimized DCAT plans achieved the planning objectives. Although target coverage was slightly better for the VMAT plans (VMAT average $PTV_r = 1.3$; DCAT average $PTV_r = 1.4$), this was not shown to be statistically significant. Similarly, average R50 values for VMAT and DCAT were very close (4.5 and 4.6, respectively). Overall, optimized DCAT plans showed inferior plan quality compared to the VMAT plans when OAR overlapped or were in close proximity to the PTV volume, but showed comparable or superior quality when targets were far from OAR.

Plans for sample lung and liver cases are shown in Figure 1.

The average number of MU in optimized DCAT plans was reduced by a factor of 2.5 compared to VMAT plans (Table 2).

All VMAT and DCAT plans were accurately delivered on a static IMRT QA phantom and had excellent gamma index passing rates, with > 95 percent of evaluated points within the gamma index criteria.

Table 2.
Average MU in VMAT and optimized DCAT plans for 19 lung and liver SBRT cases

<table>
<thead>
<tr>
<th></th>
<th>VMAT</th>
<th>Optimized DCAT</th>
<th>VMAT:DCAT ratio</th>
</tr>
</thead>
<tbody>
<tr>
<td>Average MU</td>
<td>5,548.7</td>
<td>2,277.9</td>
<td>2.52</td>
</tr>
<tr>
<td>Standard deviation</td>
<td>2,077.9</td>
<td>991.1</td>
<td>1.0</td>
</tr>
<tr>
<td>Range</td>
<td>1,647–8,062</td>
<td>948–3,955</td>
<td></td>
</tr>
</tbody>
</table>
Discussion and conclusions

With DCAT, the beam aperture is almost always open to cover the entire PTV, so the MU per fraction is reduced compared to VMAT and static IMRT deliveries. Since the number of MU correlates to delivery time, we have shown that optimized DCAT lung and liver SBRT plans could be delivered on average 2.5x faster than VMAT plans, with generally similar plan quality.

The ability to vary dose rate and gantry speed, combined with the ability to spare OAR with SSO, enables optimized DCAT to provide highly conformal dose coverage comparable to VMAT plans. Plus, since DCAT plans produce a more homogenous delivery fluence by nature, and the MLC leaves do not block the PTV during delivery, the interplay effect between MLC motion and PTV motion is minimized.

Based on the results of this study, lung and liver SBRT patients with simple, spherical lesions that are not close to OAR are ideal candidates for optimized DCAT. At our institution, this would mean that 40–60 percent of SBRT patients who would normally be treated using VMAT could be treated more efficiently using optimized DCAT, while maintaining plan quality. These patients could benefit from significantly shorter treatment times, which are easier to tolerate and reduce the risk of intrafraction movement.

VMAT would still be the preferred option for cases where OAR (such as ribs or heart in lung cases, or stomach in liver cases) are very close to or overlap the PTV.

The average DCAT MU in this study was around 2,300, which would take less than two minutes to deliver both arcs using a 6 MV FFF beam (1,200 MU/min). The shorter treatment times achieved with optimized DCAT are favorable for the deep inspiration breath hold (DIBH) technique. DIBH would further benefit patients by allowing reduced ITV and PTV volumes and improved healthy tissue sparing.

In conclusion, optimized DCAT offers faster treatments for lung and liver SBRT patients, while generally maintaining plan quality. The potential for application of optimized DCAT to other treatment sites, such as pancreas, brain and prostate, is of great interest and the subject for future investigation.
References


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